

# The Bin Area Method: A Computationally Efficient Technique for Analysis of Ventricular and Atrial Intracardiac Electrograms

ROBERT D. THRONE, JANICE M. JENKINS, and LORENZO A. DICARLO\*

From the Medical Computing Laboratory, Department of Electrical Engineering and Computer Science, University of Michigan, Ann Arbor, and the \*Cardiac Electrophysiology Laboratory, St. Joseph Mercy Hospital of the Catherine McAuley Health Center, Ann Arbor, Michigan

**THRONE, R.D., ET AL.: The Bin Area Method: A Computationally Efficient Technique for Analysis of Ventricular and Atrial Intracardiac Electrograms.** Recent studies have reported a significant false positive rate in delivery of therapy by implantable antitachycardia devices utilizing detection algorithms based on sustained high rate. More selective decision schemes for the recognition of life-threatening arrhythmias have been recently proposed that use analysis of the intrinsic electrogram rather than rate alone. Morphological discrimination of abnormal electrograms using correlation waveform analysis (CWA) has been proposed as an effective method of intracardiac electrogram analysis, but its computational demands limit its use in implantable devices. A new method for intracardiac electrogram analysis, the bin area method (BAM), was created to detect abnormal cardiac conduction with computational requirements of one-half to one-tenth those of CWA. Like CWA, BAM is a template matching method that is sensitive to conduction changes revealed in the electrogram morphology and is independent of amplitude and baseline fluctuations. Performance of BAM and CWA were compared using bipolar right ventricular and right atrial electrode recordings from 47 patients undergoing clinical cardiac electrophysiology studies. Nineteen patients had 31 distinct monomorphic ventricular tachycardias (VTs) induced (group I), thirteen patients had paroxysmal bundle branch block of supraventricular origin (BBB) induced (group II), and 19 patients had retrograde atrial activation during right ventricular overdrive pacing (group III). (One patient was common to all three groups, and two patients were common to groups II and III.) Using the ventricular electrogram, both BAM and CWA distinguished VT from sinus rhythm in 28/31 (90%) cases, and BBB from Normal Sinus Rhythm (NSR) in 13/13 (100%) patients. Using the atrial electrogram, both BAM and CWA distinguished anterograde from retrograde atrial activation in 19/19 (100%) patients. BAM achieves similar performance to CWA with significantly reduced computational demands, and may make real-time analysis of intracardiac electrograms feasible for implantable pacemakers and antitachycardia devices. (*PACE*, Vol. 13, October 1990)

pacemaker-mediated tachycardia, dual-chamber pacemaker, tachycardia, tachyarrhythmia, retrograde atrial activation

## Introduction

Recent studies have reported a significant false positive rate in delivery of therapy by im-

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This work was partially supported by NSF grant No. EET-8351215 and a grant from Medtronic, Inc.

Address for reprints: Robert D. Throne, Medical Computing Laboratory, Department of Electrical Engineering, and Computer Science, 1301 Beal Street, Ann Arbor, MI 48109-2122.

Received March 29, 1990; Revision July 19, 1990; Accepted July 19, 1990.

plantable antitachycardia devices.<sup>1-7</sup> Intracardiac electrogram analysis methods have been proposed for detecting one or more features of an atrial or ventricular electrogram for improved automated diagnosis of a specific arrhythmia, but few of these algorithms have been shown to be uniformly reliable.<sup>8-23</sup>

Correlation Waveform Analysis (CWA) has been proposed as an effective method of intracardiac waveform analysis for distinguishing ventricular electrograms during ventricular

tachycardia (VT) from those during sinus rhythm,<sup>16,19,24,25</sup> ventricular electrograms during normal sinus rhythm (NSR, QRS  $\leq$  120 msec) from those during paroxysmal bundle branch block of supraventricular origin (BBB),<sup>19</sup> and retrograde atrial activation from anterograde atrial activation.<sup>26</sup> CWA computes the correlation coefficient,  $\rho$ , between a normal template and each waveform under analysis. The correlation coefficient is independent of amplitude and baseline changes between the template and the signal under analysis, and produces a bounded index of merit between -1 and 1 (a value of 1 indicating a perfect match to the template). Although CWA is an effective method of intracardiac waveform analysis, it has the disadvantage of being a computationally demanding algorithm.

The purpose of the present study was to develop and test an innovative waveform analysis technique, the Bin Area Method (BAM), which has fewer computational demands than CWA but with a reliability similar to CWA. BAM compares corresponding areas, or bins, constructed from the template with bins constructed from subsequent depolarizations using a simple error measure. Like CWA, BAM was designed to be independent of amplitude and baseline fluctuations and to produce an index of merit between -1 and 1 where a value of 1 indicates a perfect match to the template.

In this study, BAM was used to compare ventricular electrograms during VT to those during sinus rhythm (or atrial fibrillation), ventricular electrograms during paroxysmal bundle branch block (BBB) of supraventricular origin to those during normal sinus rhythm (NSR), and atrial electrograms during 1:1 retrograde atrial activation. CWA was used as a standard against which to compare BAM for analysis of accuracy and computational requirements.

## Methods and Materials

### Electrophysiology Study

Bipolar (1 cm) atrial and ventricular endocardial electrograms were recorded during elective clinical cardiac electrophysiology studies as previously reported.<sup>16,19,26</sup> Three 6F quadrapolar

electrode catheters with an interelectrode distance of 1 cm (USCI, Billerica, MA, USA) were introduced and advanced under fluoroscopic guidance to the high right atrium (or right atrial appendage) and right ventricular apex. Two catheters were positioned in the right ventricular apex with one dedicated to pacing and the other to obtaining recordings from the distal electrode pair. All recordings were made with the patients lying supine. Ventricular electrograms were recorded on FM magnetic tape (Hewlett-Packard Models 3968 and 3964A [Hewlett-Packard, San Diego, CA, USA]) from distal bipolar endocardial electrodes positioned in the right ventricular apex using amplifiers with filter settings of 0.5 to 500 Hz (Siemens Mingograf-7 [Siemens-Elema, Solna, Sweden]) or 1 to 500 Hz (Honeywell [Denver, CO, USA] Electronics for Medicine [Pleasantville, NY, USA]). Tape speed was 3 $\frac{3}{4}$  inches/sec with a bandwidth of 0 to 1,250 Hz. For comparing the results using CWA and BAM in discriminating ventricular electrograms during ventricular tachycardia from those during sinus rhythm or atrial fibrillation (group I), ventricular electrograms were obtained from 19 consecutive patients consisting of 17 men and two women. Specific details of this patient population are given in Table I. For comparing ventricular electrograms during normal sinus rhythm with those during paroxysmal bundle branch block of supraventricular origin (group II), ventricular electrograms were obtained from 13 consecutive patients consisting of six men and seven women. Specific details of this patient population are given in Table II. For examining atrial electrograms during retrograde and anterograde atrial activation (group III), atrial electrograms were obtained from 19 consecutive patients consisting of 12 men and seven women. None of the patients had dual atrioventricular nodal pathways or accessory atrioventricular connections, and specific details of these patients are given in Table III. As Tables I-III indicate, one patient was common to all three studies, and two patients were common to two studies. Recorded endocardial electrograms were subsequently replayed and digitized on a personal computer with a Tecmar Lab Master (Scientific Solutions, Inc., Solon, OH, USA) analog-to-digital system at a sampling rate of 1,000 Hz.

**Table I.**  
Patient Data for Discriminating VT from SR/AF

Patient	Sex	Heart Disease	Drugs	Sinus Rhythm/ Atrial Fibrillation QRS Morphology	Ventricular Tachycardia QRS Morphology
1	M	CAD	None	SR-Normal	RBB-S/R
2	M	CAD	None	SR-Normal	LBB-S/L
3a	M	CAD	None	SR-LBBB	LBB-S/R
3b					LBB-S/L
4a	M	CAD	None	AF-LBBB	LBB-S/L
4b					LBB-S/L
5a	M	CAD	Proc	SR-Normal	RBB-I/R
5b					LBB-I/R
6a	M	CAD	Proc	SR-Normal	RBB-I/L
7a	F	CAD	Am	SR-Normal	RBB-S/L
7b					RBB-S/L
8	F	None	Am	SR-Normal	RBB-S/R
9	M	CAD	Qu Me	SR-Normal	LBB-S/L
10a	M	CAD	Am	SR-LBBB	LBB-S/L
11	M	VHD	Am	SR-LBBB	LBB-S/R
12	M	CAD	Am Me	SR-LBBB	LBB-I/R
13	M	CAD	En	SR-LBBB	LBB-I/L
14	M	CAD	Qu Me	SR-RBBB	RBB-S/R
15	M	CAD	Proc	SR-RBBB	LBB-S/R
16a	M	CAD	Am	SR-IVCD	RBB-I/R
16b					RBB-S/L
17	M	CAD	Am	SR-IVCD	LBB-S/L
18a	M	CAD	Am	SR-IVCD	†RBB-S/R
18b					†LBB-S/L
18c					†LBB-S/L
18d					†RBB-S/R
18e					†RBB-S/R
10b*	M	CAD	Am En	SR-IVCD	RBB-S/R
10c					LBB-I/L
6b*	M	CAD	En Proc	AF-IVCD	RBB-S/R
19	M	CAD	Qu Di	AF-IVCD	RBB-S/L

These patients were studied on two different days with two different VT morphologies. †This patient had five distinct VT morphologies. CAD = coronary artery disease; VHD = valvular heart disease; Am = amiodarone; Di = digoxin; En = encainide; Me = mexiletene, Proc = procainamide; Qu = quinidine; SR = sinus rhythm; AF = atrial fibrillation; LBBB = left bundle branch block; RBBB = right bundle branch block; IVCD = nonspecific intraventricular conduction delay; LBB = left bundle branch morphology; RBB = right bundle branch morphology; I = inferior axis; S = superior axis; L = leftward; R = rightward.

**Method of Analysis**

Data sets consisted of three passages from each patient. For discriminating ventricular electrograms during VT from those during sinus rhythm or atrial fibrillation (SR/AF), two separate ventricular passages were digitized from re-

cordings made during SR/AF, and a third passage was digitized during induced monomorphic VT. For discriminating paroxysmal bundle branch block of supraventricular origin from normal sinus rhythm, two separate ventricular passages were digitized from recordings made during NSR. The third passage was digitized from recordings

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**Table II.**

Patient Data for Discriminating Paroxysmal Bundle Branch Block  
of Supraventricular Origin from Normal Sinus Rhythm

Patient	Sex	Heart Disease	Drugs	Method of BBB Induction	Aberration Morphology
20	F	None	None	Spontaneous	RBBB
21	F	None	None	AOP	RBBB
22	F	None	None	AOP	RBBB
8	F	None	None	Spontaneous	RBBB
23	F	None	Iso	AOP	RBBB
24	F	None	Iso	Atrial Fibrillation	RBBB
25	F	None	Iso	Spontaneous	RBBB
26	M	COPD	None	AOP	RBBB
27	M	CAD	None	Spontaneous	RBBB
28	M	CAD	None	AOP	RBBB
29	M	CAD	Proc	AOP	RBBB
30	M	None	Iso	AOP	LBBB
31	M	CAD	None	AOP	LBBB

CAD = coronary artery disease; COPD = chronic obstructive pulmonary disease; Iso = isopril; Proc = procainamide; LBBB = left bundle branch block; RBBB = right bundle branch block; AOP = atrial overdrive pacing.

**Table III.**

Patient Data for Discriminating Retrograde from Anterograde Atrial Activation

Patient	Sex	Heart Disease	Drugs	Atrial Electrode Location
23	F	None	Iso	RAA
32	M	None	None	RAA
33	M	None	None	RAA
34	F	None	None	RAA
35	M	CAD	None	RAA
36	M	None	None	RAA
37	M	None	None	RAA
38	F	None	None	RAA
26	M	COPD	None	RAA
39	F	None	None	RAA
40	M	CAD	None	RAA
41	M	CAD	Ve	RAA
8	F	None	None	RAA
42	M	None	None	RAA
43	F	None	None	HRA
44	M	None	Qu Ve	HRA
45	M	None	None	HRA
46	F	None	Ep	HRA
47	M	None	En	HRA

En = encainide; Ep = epinephrine; Iso = isopril; Qu = quinidine; Ve = verapamil; CAD = coronary artery disease; COPD = chronic obstructive pulmonary disease; RAA = right atrial appendage; HRA = high right atrium.

made during BBB. For discriminating retrograde from anterograde atrial activation, two separate atrial passages were digitized from recordings made during sinus rhythm (anterograde atrial activation) and a third passage during retrograde atrial activation while pacing the right ventricle at a rate sufficient to maintain 1:1 retrograde conduction to the atrium.

In all cases, the initial passage of SR/AF, NSR, or anterograde atrial activation was used to construct a ventricular or atrial electrogram template by signal averaging. The template was employed for subsequent comparison with a second separate SR/AF, NSR, or anterograde control passage and a later passage of either VT (group I), BBB (group II), or retrograde atrial activation (group III). A careful selection of window size effectively excluded any local repolarization in order to avoid the inclusion of injury current caused by temporary endocardial damage adjacent to the catheter.<sup>19,26</sup> A software trigger (peak detector) was used for automatic recognition of each of the sequential waveforms.<sup>16,19,26</sup> An algorithm was declared successful if there was no overlap in the ranges of the similarity values  $\rho$  during the abnormal passage when compared to the ranges during the normal passage.

In presenting both CWA and BAM, the following notation will be used.

- N = the number of points in the template.
- $t_i$  = the template points.
- $s_i$  = the signal points to be processed.
- $\bar{t}$  = the template average.
- $\bar{s}$  = the signal average.

**CWA**

The correlation coefficient,  $\rho$ ,<sup>16,19,26</sup> is independent of amplitude and baseline fluctuations between the template and waveform under analysis and produces an output between -1 and 1. Mathematically, the correlation coefficient is defined as:

$$\rho = \frac{\sum_{i=1}^{i=N} (t_i - \bar{t})(s_i - \bar{s})}{\sqrt{\sum_{k=1}^{k=N} (t_k - \bar{t})^2} \sqrt{\sum_{k=1}^{k=N} (s_k - \bar{s})^2}}$$

For comparison with the similarity measure used in BAM, the correlation coefficient is equivalent to the following squared-error norm:

$$\rho = 1 - \frac{1}{2} \sum_{i=1}^{i=N} \left( \frac{t_i - \bar{t}}{\sqrt{\sum_{k=1}^{k=N} (t_k - \bar{t})^2}} - \frac{s_i - \bar{s}}{\sqrt{\sum_{k=1}^{k=N} (s_k - \bar{s})^2}} \right)^2$$

To avoid the square-root computation, we can equivalently compute

$$\rho = \rho^2 \text{ sign}(\rho)$$

where sign returns the arithmetic sign of the argument ( $\pm 1$ ).

**BAM**

BAM compares corresponding areas or bins constructed from the template with bins constructed from subsequent depolarizations using a simple error measure. Consecutive sample points are summed to estimate the areas using a rectangular area rule in equal sized bins. The average of these bin values (DC offset) is then removed resulting in a correction of baseline shift, and then these corrected bin values are normalized by the absolute sum of all corrected bin values. As a final step, the sum of the absolute difference of these normalized and corrected bins with an identically processed template is computed.

To compute bin areas, we add consecutive sample points. To form 5-point bins,

$$\begin{aligned} S_1 &= s_1 + s_2 + s_3 + s_4 + s_5 \\ S_2 &= s_6 + s_7 + s_8 + s_9 + s_{10} \\ &\vdots \\ S_M &= s_{N-4} + s_{N-3} + s_{N-2} + s_{N-1} + s_N \end{aligned}$$

To form three-point bins,

$$\begin{aligned} S_1 &= s_1 + s_2 + s_3 \\ S_2 &= s_4 + s_5 + s_6 \\ &\vdots \\ S_M &= s_{N-2} + s_{N-1} + s_N \end{aligned}$$

To form one-point bins,  $S_i = s_i$ ,  $i = 1, \dots, N$ . Template points,  $t_i$ , are processed similarly to form the  $T_i$ . For M equally sized bins in the template, the index of merit for BAM is given as

$$\rho = 1 - \sum_{i=1}^{i=M} \left| \frac{T_i - \bar{T}}{\sum_{k=1}^{k=M} |T_k - \bar{T}|} - \frac{S_i - \bar{S}}{\sum_{k=1}^{k=M} |S_k - \bar{S}|} \right|$$

where  $\bar{S} = \frac{1}{M} \sum_{k=1}^{k=M} S_k$ , and  $\bar{T} = \frac{1}{M} \sum_{k=1}^{k=M} T_k$ .

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Table IV.

Alignment	CWA	BAM			Total Tested
		1 pt	3 pt	5 pt	
VT vs. SR/AF (Group I)					
Original (Peak)	27	26	25	25	31
Best Fit	28	28	28	26	31
BBB vs. NSR (Group II)					
Original (Peak)	13	13	13	13	13
Best Fit	13	13	13	13	13
RAA vs. AAA (Group III)					
Original (Peak)	14	15	16	14	19
Best Fit	19	19	19	19	19

Results for discriminating ventricular tachycardia from sinus rhythm/atrial fibrillation (VT vs SR/AF, Group I), paroxysmal bundle branch block from normal sinus rhythm (BBB vs NSR, Group II), and retrograde from antero-grade atrial activation (RAA vs AAA, Group III) at both the original and best fit trigger locations. The numbers in the rows indicate the number of instances in which the ranges of  $r$  for the normal depolarizations did not overlap with the ranges of  $r$  for the abnormal depolarizations for the total tested number of passages.

Because of the design of BAM, all template processing is performed in advance, i.e., prior to analysis of incoming depolarizations subject to analysis. BAM requires one-half the multiplications of CWA for 1-point bins, one-sixth the multiplications of CWA for three-point bins, and one-tenth the multiplications for five-point bins. Note that we need to compute  $1/\sum_{k=1}^M |S_k - \bar{S}|$  only once. After that we only need to do multiplications which involve less computation time than divisions in the type of microprocessors likely to be used in an implantable device. BAM is similar to area of difference (AD),<sup>13,14,18</sup> but is designed to be independent of amplitude and baseline fluctuations.

Triggering

The true (ideal) performance for any template matching algorithm requires precise alignment between the template and current waveform under analysis. However, in an implantable device a peak detector or slope detector with alignment at a single point is more likely. In order to examine the effect of trigger alignment on performance, BAM and CWA were computed using

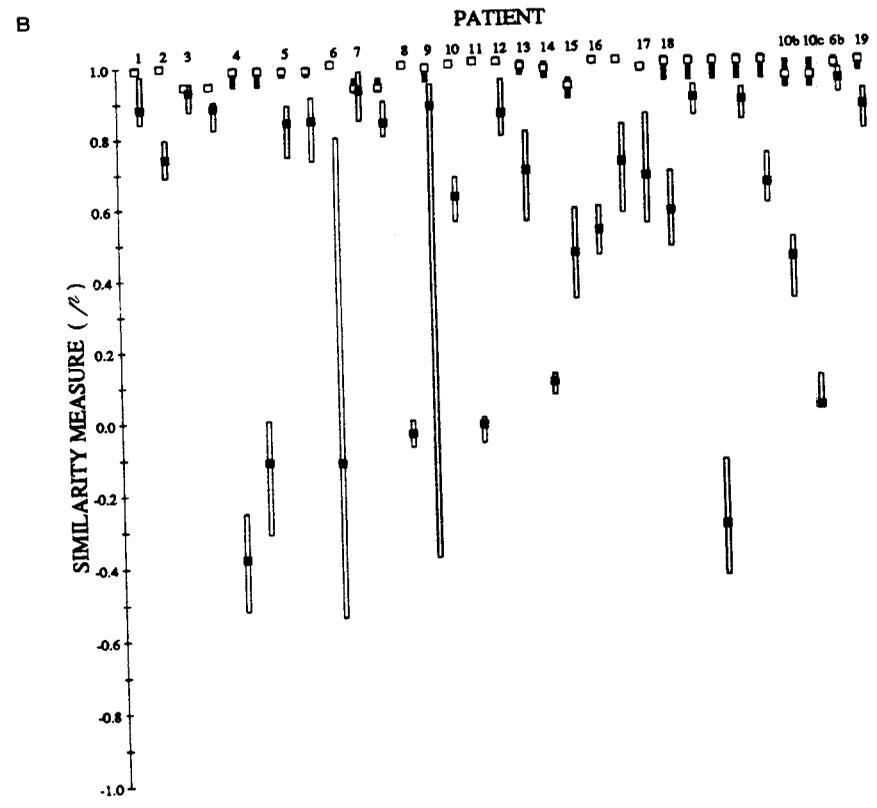
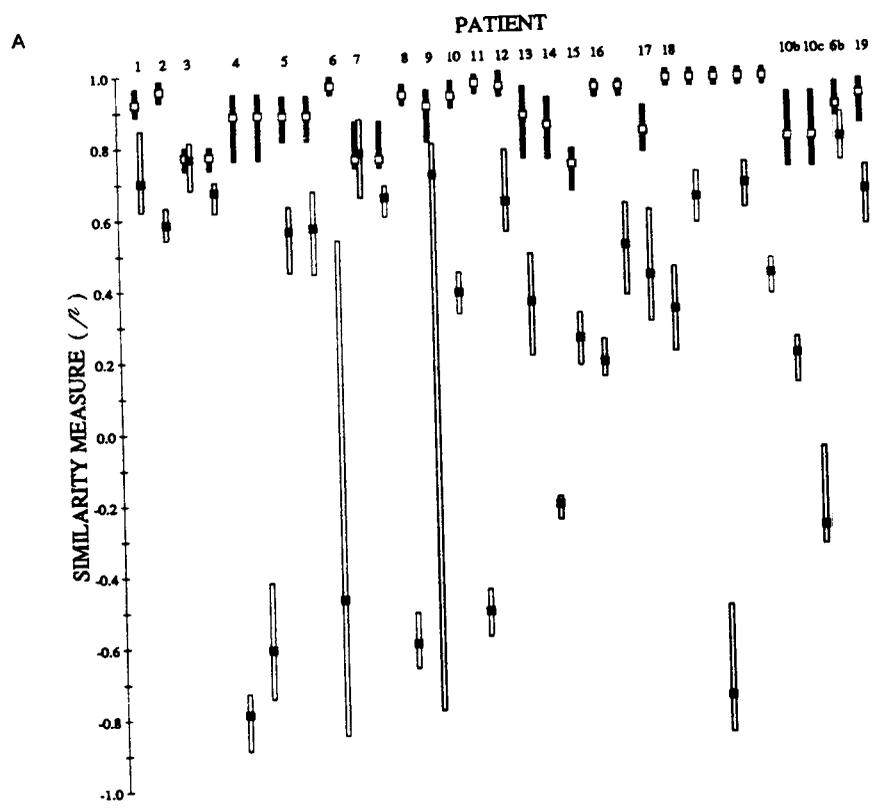
both a peak amplitude trigger (original) and a best fit alignment between template and waveform under analysis within an 11 msec window of the original trigger location as previously described.<sup>19,26</sup>

Results

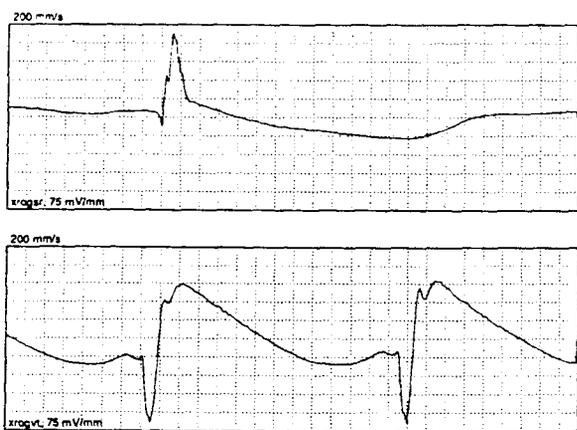
For either method, BAM or CWA, there is no universal threshold which will separate VT from SR/AF, BBB from NSR, or retrograde from antero-grade atrial activation in the patient population studied. Instead, patient specific thresholds were required for each method. Results for groups I, II, and III are summarized in Table IV for both the original and the best fit triggers. In some instances, while there was no overlap in the ranges and an algorithm was declared successful, the ranges of similarity measures during the abnormal and corresponding normal passages were very close.

Detecting Ventricular Tachycardia (Group I)

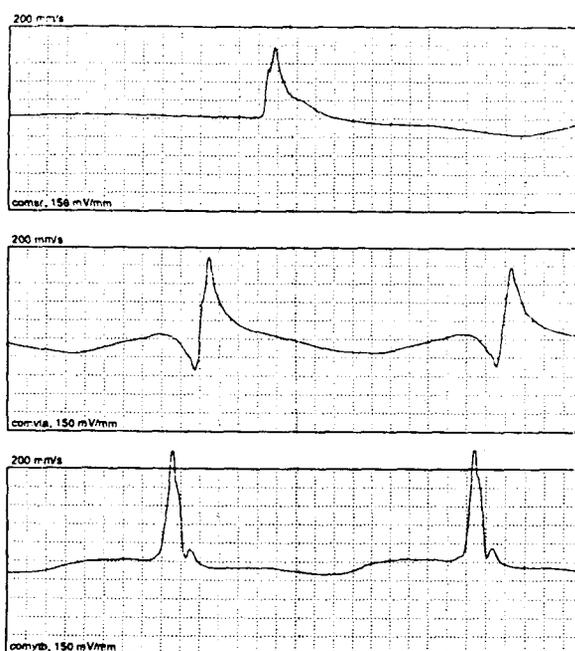
Figure 1 summarizes results using BAM with three-point bins (panel A) and CWA (panel B) at



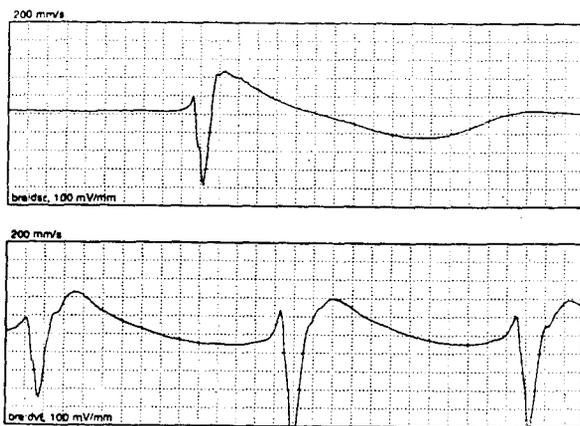
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**Figure 2.** Ventricular electrograms during sinus rhythm (top) and ventricular tachycardia (bottom) for patient 8. Both electrograms are displayed at 200 mm/sec and at the same scale. (The dotted lines represent 5 mm.) Both BAM and CWA could easily distinguish all ventricular tachycardia depolarizations from all sinus rhythm depolarizations for this patient.



**Figure 4.** Ventricular electrograms during sinus rhythm (top) and two distinct ventricular tachycardia morphologies for patient 7. Both electrograms are displayed at 200 mm/sec and at the same scale. (The dotted lines represent 5 mm.) Both BAM and CWA failed to distinguish all of the ventricular tachycardia depolarizations during the passage of the first VT morphology (middle passage), but both distinguished all depolarizations of the second VT from sinus rhythm.



**Figure 3.** Ventricular electrograms during sinus rhythm (top) and ventricular tachycardia (bottom) for patient 12. Both electrograms are displayed at 200 mm/sec and at the same scale. (The dotted lines represent 5 mm.) Both BAM and CWA could distinguish all ventricular tachycardia depolarizations from all sinus rhythm depolarizations for this patient.

the best fit location in discriminating VT from SR/AF. Using the original trigger, BAM with one-, three-, and five-point bins discriminated VT from SR/AF in 26/31 (84%), 25/31 (81%), 25/31 (81%) cases, while CWA discriminated VT from SR/AF in 27/31 (87%) cases. Using the best fit alignment, BAM with one-, three- and five-point bins discriminated VT from SR/AF in 28/31 (90%), and 28/31 (90%), and 26/31 (84%) instances, while CWA discriminated VT from SR/AF in 28/31 (90%) cases.

Figures 2, 3, and 4 display ventricular electrograms during both sinus rhythm and mono-

**Figure 1.** Results of BAM with three-point bins (A) and CWA (B) using the best fit alignment for distinguishing VT from SR (group I). The ranges of  $\rho$  during SR/AF are shown in white, with a black box at the mean, while the ranges of  $\rho$  for VT are shown in black, with a white box at the mean.

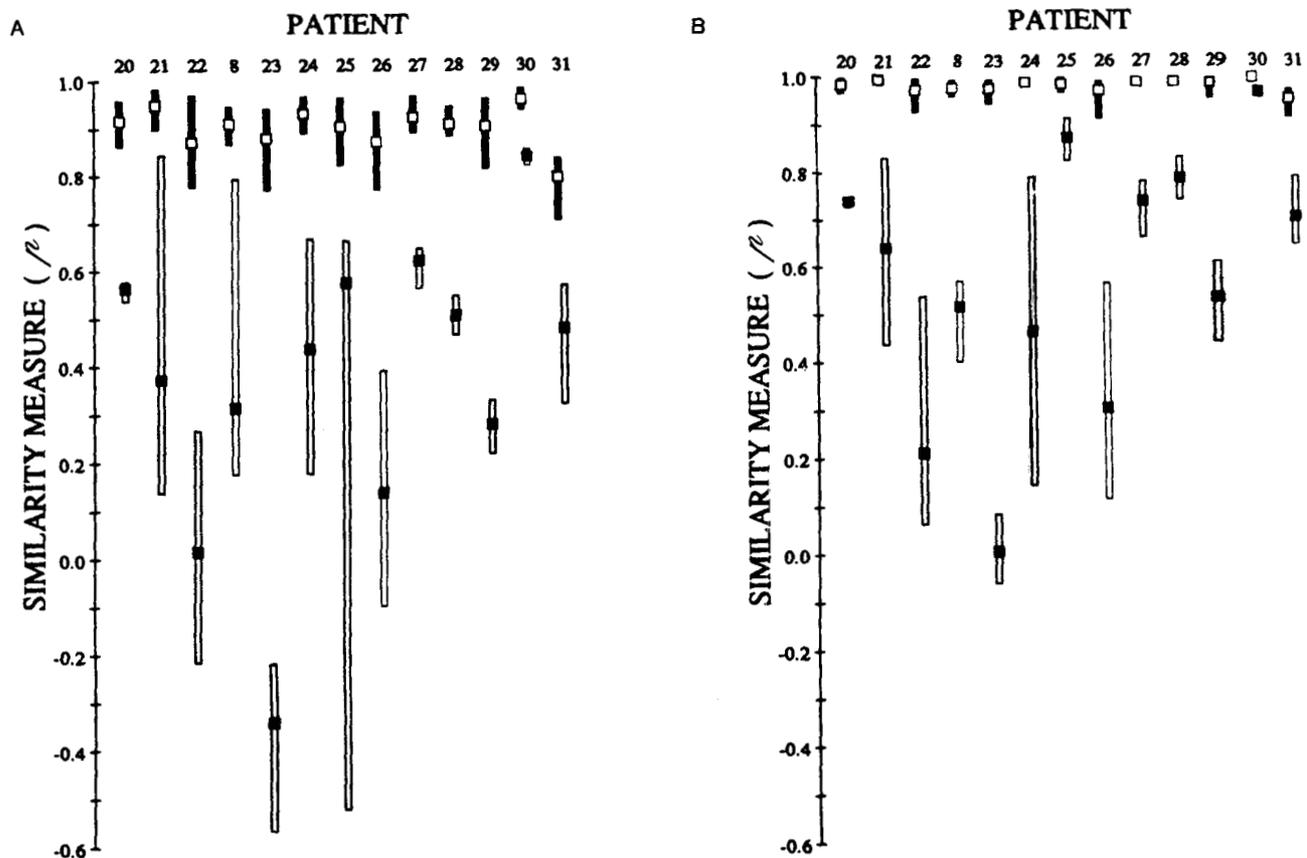
morphic ventricular tachycardia for patients 8, 12, and 7. All electrograms are played at 200 mm/sec and at the same scale. For patient 8 (Fig. 2) the electrograms during both sinus rhythm and VT are easily distinguishable for both BAM and CWA. For patient 12 (Fig. 3), both BAM and CWA could distinguish VT from SR, even though the electrograms appear quite similar. For patient 7 (Fig. 4), both BAM and CWA could not distinguish the first VT from SR, but both could distinguish the second VT. While it may appear that the ventricular electrograms during the first VT look different than during SR, the template was chosen based on the SR depolarization only, and was chosen to begin when SR depolarization began. Thus the earlier activation during the first VT was not included.

**Detecting Paroxysmal Bundle Branch Block (Group II)**

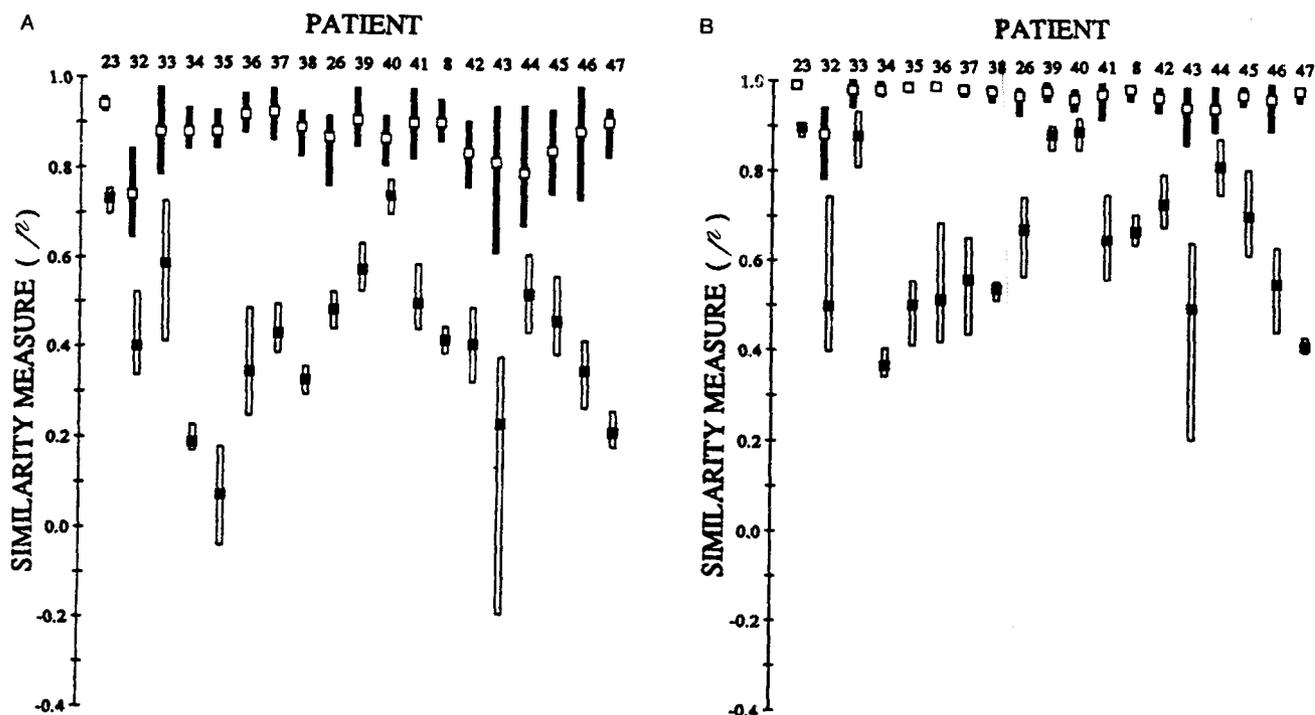
Figure 5 summarizes results of using BAM with three-point bins (panel A) and CWA (panel B) at the best fit location in discriminating BBB from NSR. Using the original trigger, both BAM with one-, three-, and five-point bins and CWA discriminated BBB from NSR in 13/13 (100%) patients. Using the best fit alignment, both BAM with one-, three-, and five-point bins and CWA discriminated BBB from NSR in 13/13 (100%) patients.

**Detecting Retrograde Atrial Activation (Group III)**

Figure 6 summarizes results using both BAM with three-point bins (Panel A) and CWA (panel



**Figure 5.** Results of BAM with three-point bins (A) and CWA (B) using the best fit alignment for discriminating BBB from NSR (Group II). The ranges of  $r$  during NSR are shown in white, with a black box at the mean, while the ranges of  $r$  for BBB are shown in black, with a white box at the mean.



**Figure 6.** Results of BAM with 3-point bins (A) and CWA (B) using the best fit alignment for distinguishing RAA from AAA (group III). The ranges of  $\rho$  during anterograde atrial activation (AAA) are shown in white, with a black box at the mean, while the ranges of  $\rho$  for retrograde atrial activation (RAA) are shown in black, with a white box at the mean.

B) using the best fit location for separating retrograde atrial activation from anterograde atrial activation. Using the original trigger BAM with one-, three-, and five-point bins discriminated anterograde from retrograde atrial activation in 15/19 (79%), 16/19 (84%), and 14/19 (74%) patients, while CWA discriminated anterograde from retrograde ranges in 14/19 (74%) patients. Using the best fit alignment, both BAM with one-, three-, and five-point bins and CWA discriminated retrograde from anterograde atrial activation in 19/19 (100%) patients.

### Discussion

Overall, the results for BAM in discriminating VT from sinus rhythm/atrial fibrillation, BBB from normal sinus rhythm, and retrograde from anterograde atrial activation, were similar to those of CWA. In detecting VT, CWA was slightly superior to BAM at the original trigger location. The results using BAM with one- and three-point

bins were identical to those of CWA at the best fit location. In discriminating BBB from NSR, both BAM with one-, three-, and five-point bins and CWA were successful in 13/13 (100%) cases at both the original and best fit trigger locations. In detecting retrograde from anterograde atrial activation, BAM with one-, and three-point bins was slightly superior to CWA at the original trigger. Both methods detected all retrograde atrial activation using the best fit trigger location.

As indicated in Figures 1, 5, and 6, ranges of values for CWA are generally smaller than those using BAM, while mean values are generally better separated using BAM than CWA. Given the reduced computational requirements of BAM, this separation of the mean values (typically used as a performance measure) is an important consideration.

While CWA has been successful in discriminating VT from sinus rhythm,<sup>16,19,24</sup> paroxysmal BBB of supraventricular origin from normal sinus rhythm,<sup>19</sup> and retrograde from anterograde atrial

activation,<sup>26</sup> it has the potential disadvantage of being too computationally demanding for use in an implantable device. One alternative method, AD,<sup>13,14,18</sup> has been shown to discriminate ventricular electrograms during VT from those during sinus rhythm, and to differentiate ventricular electrograms during paroxysmal bundle branch block from those of sinus rhythm with a normal QRS<sup>19</sup> with much lower computational cost than CWA. However, in contrast to CWA and BAM, the results using AD may be adversely affected by amplitude changes.<sup>18</sup>

### Conclusion

Rapid and reliable digital analysis of intracardiac electrograms may significantly increase the specificity of detection of pathological tachycardia by implantable antitachycardia devices without sacrificing sensitivity. We present the

design of a new algorithm, BAM which like CWA is a template matching technique independent of amplitude or baseline fluctuations between the template and each waveform under analysis. BAM has been shown to be reliable in intracardiac waveform analysis, and compares favorably with correlation waveform analysis at considerably reduced complexity. Depending on the size of the bins used, BAM requires from one-half to one-tenth the multiplications of CWA. BAM may make real-time morphology analysis of intracardiac electrograms feasible for antitachycardia devices.

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*Acknowledgments:* The authors wish to express their appreciation to Colleen Hoover, B.S., Barbara Nagrant, C.V.R.T., and Judy Jaffke, R.T. (R), for their technical assistance in the cardiac electrophysiology laboratory, and Ms. Debbie Laird for preparation of this manuscript.

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